



Microwave-assisted synthesis of localized surface plasmon resonance enhanced bismuth selenide (Bi₂Se₃) layers for non-enzymatic glucose sensing



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ABSTRACT

Three-dimensional (3D) bismuth selenide (Bi₂Se₃) nanostructures were synthesized by microwave synthesis using water as a solvent and hydrazine hydrate as a reducing agent and exfoliated into few layers of Bi₂Se₃. Bi₂Se₃- Few Layers (Bi₂Se₃- FL) exhibited localized surface plasmon resonance and enhanced electrocatalytic behavior. The scanning electron microscope (SEM) and transmission electron microscopy (TEM) characterization indicated the layered structure of Bi₂Se₃. The electrocatalytic properties of the Bi₂Se₃-FL modified GC electrode towards non-enzymatic glucose oxidation were evaluated by cyclic voltammetry (CV) and chronoamperometry. The designed non-enzymatic glucose sensor showed a low detection limit of 6.1 μM, a linear range from 10 μM to 100 μM of glucose concentration and a current sensitivity of 0.112 μA μM⁻¹. The electrochemical sensor constructed using Bi₂Se₃-FL attained steady-state level within 3 s upon adding glucose and remained stable even after 19 days with only 17% loss in current signal. The obtained electrodes can be applied for determining glucose in urine samples. The results obtained here are of great significance to use nanostructured Bi₂Se₃-FL electrode as a potential candidate for non-enzymatic glucose detection.

1. Introduction

In human body glucose present in the blood is a vital source of energy to supply energy for the daily activities. When the glucose content in the blood exceeds requirements, the excess glucose causes diabetes mellitus, a common disease that can result in disability and death [1]. Ever since the discovery of the first enzyme based electrochemical glucose biosensor in 1962 by Clark et al., there have been constant efforts by the researchers to replace enzymatic electrochemical biosensors due its high cost, difficulty in enzyme immobilization process and decline in the activity of enzymes, irrespective of its high selectivity and sensitivity [1–3]. In pursuit of identifying cost-effective catalysts for non-enzymatic

glucose electro oxidation several catalysts have been reported including layered materials such as graphene [4] metal nitrides [5] and metal chalcogenides [6]. Since the transition metal based catalysts are less preferred owing to decreased specific area from close packing and poor conductivity, the non-enzymatic glucose detection mostly comprised of hybrid materials involving complex procedure and effective grafting. Therefore, careful engineering of the catalyst possessing large surface area and ample active sites along with structural stability are the prerequisites for ideal performance [7]. There are several attempts on investigating the electrochemical detection of glucose using pristine forms of layered materials although bismuth selenide (Bi₂Se₃) is almost unexplored.

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Bi_2Se_3 is a well-known semiconducting metal chalcogenides of the V-VI groups having potential applications in optoelectronics, thermoelectronic devices and infrared spectroscopy [8]. Bi_2Se_3 is one of the layered semiconducting materials with a narrow bandgap and tetradymite structure with space group $D^5_3d(R\bar{3}m)$. Its electronic structure with the existence of six valley degeneracy and narrow bandgap makes it suitable for optical and photosensitive device applications [9–12]. Even though Bi_2Se_3 has been synthesized in the form of nanoparticles [13], nano films [14], nanotubes [15], nanobelts [16], heterostructured nanowires [17] and layers [18] by a variety of methods [9], obtaining layered structures with high surface area to volume ratio will be desired for sensing ensuring better electrocatalytic activity.

Traditional synthesis methods do involve slow heating [19], while in microwave method the electric field supplies a force on the charged particles that makes them either to rotate or migrate and these movements result in further polarization. The electric and magnetic components of the microwaves drastically change in direction and the microwave energy provides the heat in different parts of the reaction mixture [20]. Therefore microwave heating is an advantageous synthesis technique as compared to the other conventional techniques since it supplies rapid internal volumetric heating by direct transmission with efficient and quick energy transfer into the molecules present in the reaction mixture [21]. This results in uniform increase of solution's temperature, reduced reaction time, saving of energy [22–24] and increase in the product yield [25] and rate constant as well [26]. Although significant efforts have been devoted towards the synthesis of hierarchical nanostructured bismuth selenide, most attempts involve either complicated multistep process using expensive precursors and solvents. Several works on microwave-assisted synthesis of Bi_2Se_3 with different structures and morphology such as nanoparticles [13,20] nanocrystals [13] and nanosheets [9] have been already reported in the literature.

In this report, we present a simple synthetic route to obtain layered bismuth selenide by microwave irradiation using water as a solvent. Herein we use hydrazine hydrate (N_2H_4) for its dual role, as a reducing agent and as a surfactant. The as-prepared Bi_2Se_3 -Bulk (Bi_2Se_3 -B) exhibits its absorption in the near-infrared (NIR) region suggesting the presence of localized surface plasmon resonance (LSPR). This phenomenon is usually found to occur in noble metals such as gold and silver, doped semiconductors or graphene where the surface-bound collective excitations of free charge carriers can involve in very strong light-matter interactions [27–29]. LSPR exists from the ultraviolet region to near-infrared and this will occur when the materials are in nanoscale due to quantum confinement that quantizes topological surface states [30]. The exfoliated Bi_2Se_3 -FL possess a larger surface area than its 3D bulk counterparts (Bi_2Se_3 -B). The increased surface area and high carrier density combinedly boost the electrocatalytic nature of the material. Therefore, we have attempted to investigate the LSPR enhanced nanostructured Bi_2Se_3 -FL for non-enzymatic glucose sensing. In this report, highly stable and ultrasensitive non-enzymatic glucose sensor developed using Bi_2Se_3 -FL nanostructures, synthesized and exfoliated by cost-effective wet-chemical route is presented. In recent years noble metals, and their oxides nitrides, hydroxides and phosphides have received intense research attention towards glucose electrooxidation due to their electro catalytic properties [1,5,7,31–33]. To the best of our knowledge, glucose sensing studies for graphene like nanostructured Bi_2Se_3 -FL have not been explored yet. The formation mechanism, the potential influence of 2D structure and LSPR on the resulting electrocatalytic activity have been discussed in detail. Bi_2Se_3 -FL with sheet like surface offer more active sites whereby the electrochemical performance is enhanced towards the detection of glucose with pronounced stability over long period of time. The non-enzymatic glucose sensor constructed using Bi_2Se_3 -FL exhibited a low detection limit of $6.1 \mu\text{M}$ and a linear range between $10 \mu\text{M}$ and $100 \mu\text{M}$ of glucose concentration with a current sensitivity of $0.112 \mu\text{A}\mu\text{M}^{-1}$. In addition, the electrochemical sensor showed an appreciable stability beyond 19 days with a minimal loss of 17% suggesting the suitability of Bi_2Se_3 -FL for non-enzymatic glucose

sensing.

2. Experimental part

2.1. Materials

Bismuth nitrate pentahydrate, ($\text{Bi}(\text{NO}_3)_3 \cdot 5\text{H}_2\text{O}$), Hydrazine hydrate (N_2H_4), Selenium (Se) powder, Sodium sulfite (Na_2SO_3), Glucose, Uric acid (UA), Ascorbic acid (AA), Potassium Ferricyanide ($\text{K}_3[\text{Fe}(\text{CN})_6]$), Sodium phosphate dibasic (Na_2HPO_4), Sodium phosphate monobasic (NaH_2PO_4), Nafion and Ethanol, were purchased from Sigma Aldrich Corporation. All chemicals were of reagent grade. Milli-Q water was used to prepare the aqueous solutions for the experiments.

2.2. Preparation of sodium selenosulfate (Na_2SeSO_3)

Since the pristine Selenium (Se) is not water-soluble and does not react efficiently in its pristine form, sodium selenosulfate (Na_2SeSO_3) was prepared using the procedures from our earlier report [34]. Solutions of 0.2 M selenium (Se) and 0.4 M of sodium sulfite (Na_2SO_3) were prepared and transferred to a round bottom flask followed by adding deionized (DI) water. This solution was refluxed for a period of 2 h at 125°C – 130°C using an oil bath set up to obtain Na_2SeSO_3 . The solution was filtered and used as Se source for the preparation of nanostructured 3D Bi_2Se_3 layers.

2.3. Material characterization

The prepared bismuth selenide was characterized by using powder X-ray diffraction (XRD) technique (Bruker, D4 Endeavor) with a diffraction angle of (2θ) in the range of 10° – 90° to identify the crystalline nature of the material. X-ray photoelectron analysis was carried out using Kratos Axis Ultra DLD X-ray photoelectron spectrometer with monochromatic Al $K\alpha$ (1486.708 eV) radiation. The Surface morphology was characterized using scanning electron microscope (SEM, JEOL JSM-6380 LV), CSI Nano-Observer AFM and transmission electron microscope (TEM, JEOL JEM 1200 EXII) while the optical measurements were carried out through absorption spectroscopy by using Shimadzu UV-Vis 2600 spectrometer. All electrochemical measurements were performed in a three-electrode electrochemical cell using a CHI 6044E workstation (CHI Instruments, USA). All experiments were conducted at room temperature.

2.4. Microwave synthesis of Bi_2Se_3 -FL and exfoliation

0.072 M Bismuth nitrate pentahydrate ($\text{Bi}(\text{NO}_3)_3 \cdot 5\text{H}_2\text{O}$) was added to a beaker containing 25 mL of DI water and stirred for 15 min. To this 25 mL of Na_2SeSO_3 solution was added in drops followed by the addition of 1 mL of Hydrazine hydrate (N_2H_4). The above said reaction mixture was further stirred for 30 min and subjected to microwave irradiation for 5 min. The resultant black precipitate containing layered Bi_2Se_3 -B was centrifuged several times using DI water until neutral pH was reached followed by washing with absolute ethanol and then dried in a vacuum oven at 60°C for 12 h. 1 mg of the as-prepared Bi_2Se_3 -B was added to a vial containing 10 mL of ethanol and water mixture (3:2 v/v). The dispersion was sonicated for 4 h and centrifuged to obtain the Bi_2Se_3 -FL.

2.5. Electrochemical investigation

A 10 mL glass electrochemical cell containing three electrodes was used for the electrochemical investigation. In a typical experiment a glassy carbon (GC) disk electrode was used as a working electrode (3 mm diameter) while a platinum wire, and Ag/AgCl (saturated KCl) electrodes were used as the auxiliary and reference electrodes, respectively. Prior to modification, the GC was polished with a polishing cloth, using 3.0, 1.0 and $0.05 \mu\text{m}$ alumina slurries, rinsed thoroughly with ultrapure water, and sonicated in a mixture of ethanol and water (1:1 v/v) for 5 min. 1 mg

of Bi_2Se_3 -B was measured accurately and uniformly dispersed in 10 mL of ethanol water mixture and sonicated for 10 min to obtain uniform dispersion. A volume of 10 μL of Bi_2Se_3 -B solution was drop casted on previously cleaned GC and dried at room temperature to fabricate Bi_2Se_3 -B/GC electrode. Similarly, 10 μL of Bi_2Se_3 -FL obtained using the above said procedure was drop casted on a previously cleaned GC and dried at room temperature to fabricate Bi_2Se_3 -FL/GC electrode. For real sample analysis, human urine was obtained from a healthy volunteer. The urine sample was analyzed directly without any pretreatment and was stored in the refrigerator at low temperature until the completion of all analysis. About 20 mL was centrifuged at 8000 rpm for 10 min at room temperature in order to separate the liquid in the urine from solid components such as mineral crystals, blood cells or microorganism.

3. Result and discussion

3.1. Characterization of synthesized Bi_2Se_3

Bi_2Se_3 are layered materials possessing rhombohedral crystal structure of the space group D3d (R3m). Every layer is made of five monoatomic sheets called quintuple layer (QL) and the atoms in a sheet are covalently bonded in the order of X-Bi-X-Bi-X where X = Se or Te [18]. The phase purity and crystal structure of the as-prepared 3D Bi_2Se_3 layers were examined by powder X-ray diffraction and the respective spectrum is presented in Fig. S1. In Fig. S1 (see Supporting information), the absence of characteristic peaks corresponding to impurities suggests that the final product is highly pure with certain amount of crystalline nature. The signature peaks in the pattern ((015), (110), (0015) and (205)) can be assigned to the reflection of Bi_2Se_3 rhombohedral phase (symmetry R3m) of preferential orientation of the crystallites owing to its layered structure ($a = b = 4.1396 \text{ \AA}$, $c = 28.6360 \text{ \AA}$, $\alpha = \beta = 90^\circ$, $\gamma = 120^\circ$, ICDD 33-0214)

[35,36].

Fig. 1 (A), shows the UV-vis absorbance spectrum of Bi_2Se_3 -B, dispersed in ethanol: water (3:2) mixture at room temperature. From the spectrum, it is evident that there are three broad peaks at 296 nm, 671 nm and 789 nm. The absorption in the region beyond 900 nm provides an evidence for the presence of LSPR [35,37], which would reflect in the electrocatalytic activity of this material. The LSPR phenomenon is usually encountered in noble metals in nanoscale when they interact with light and it is characterized by surface-bound charge densities in resonance with driving magnetic field [38]. Surface plasmon resonance is found in semiconductors with free carrier densities due to self-doping causing cation vacancies. These free carrier concentration are usually tuned by doping, temperature and/or phase transition [38-40].

X-Ray photoelectron spectroscopy (XPS) was carried out in order to investigate the chemical composition of the as-synthesized Bi_2Se_3 -B. The full-range survey scan spectrum (Fig. 1 (B)), exhibits peaks corresponding to Bi and Se peaks confirm the presence of Bi and Se. There are also two other peaks observed corresponding to O and C indicating the presence of O and C which is due to moisture uptake and surface hydrocarbon contaminants [41]. The absence of peaks pertaining to other elements except Bi, Se, O and C ensures the high purity of the product. The high-resolution core spectrum of Bi 4f is shown in Fig. 1 (C), which can be fitted with Bi $4f_{7/2}$ and $4f_{5/2}$ peaks located at 157.6 eV and 162.7 eV respectively [42]. Similarly Fig. 1 (D), shows the high-resolution core spectrum of Se 3d which deconvoluted in to two peaks for Se $3d_{5/2}$ and $3d_{3/2}$ with binding energies of 54.7 and 57.5 eV respectively. Apart from this there is a Selenium oxide (SeO_x) peak observed at 62.1 eV owing to the oxidation of selenium over a prolonged period of time even though the synthesized Bi_2Se_3 was not exposed to air [43].

Fig. 2 (A) shows the SEM image of the layered Bi_2Se_3 -B, while Fig. 2 (B) shows the SEM image of Bi_2Se_3 -FL obtained after exfoliation. From

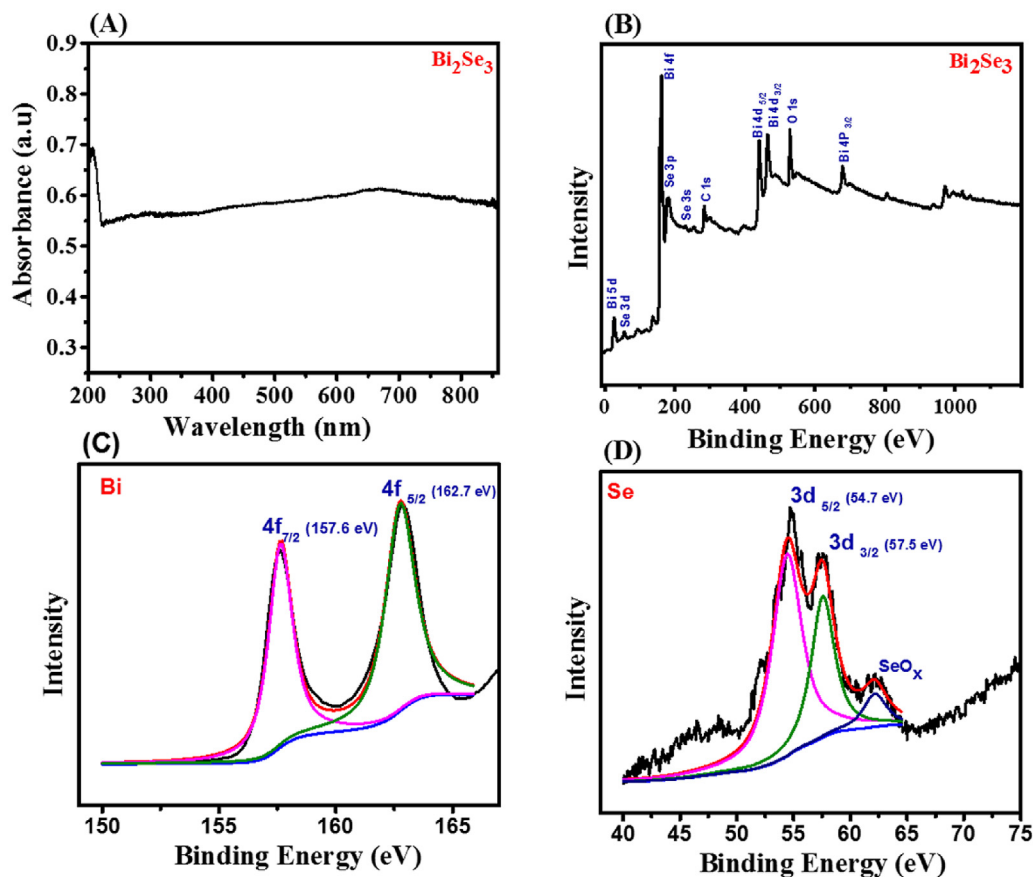


Fig. 1. (A) V-vis absorption spectra of as-synthesized Bi_2Se_3 -B; (B) XPS survey scan of Bi_2Se_3 -B; Core level XPS spectra of (C) Bi in Bi_2Se_3 -B and (D) Se in Bi_2Se_3 -B.

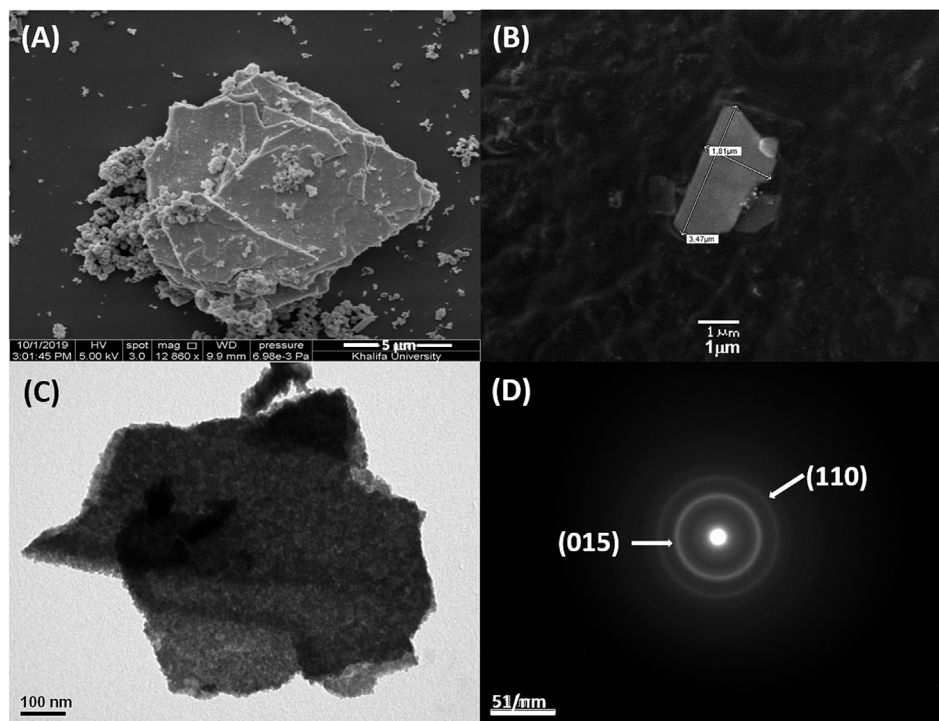


Fig. 2. SEM image of (A) as-synthesized Bi_2Se_3 -B; (B) Bi_2Se_3 -FL; (C) TEM image of Bi_2Se_3 -FL and (D) Selected area electron diffraction (SAED).

the SEM images, it can be clearly understood that the synthesized Bi_2Se_3 does possess irregular layered structures and the layers are stacked together. It is also evident that as-synthesized Bi_2Se_3 has mostly layered structures and not particles or rods. The layered structures obtained in this work have been achieved using water as a solvent, without the addition of any surfactant or ionic liquids. The Bi_2Se_3 -FL obtained by exfoliation Fig. 2 (B) are found few μm in width, ensuring large surface to volume ratio, which increases the density of free carriers [35]. The EDS analysis and elemental mapping exhibit the presence of Bi and Se in the compound synthesized and their uniform distribution throughout respectively (Fig. S2 (see Supporting information)).

Fig. 2(C) and (D), display TEM micrograph of Bi_2Se_3 -FL and its corresponding selected area electron diffraction (SAED) respectively. The TEM image reveals that the exfoliated Bi_2Se_3 -FL consist of stacked few layers as compared to Bi_2Se_3 -B (Fig. 2(A)). From the TEM images, it is evident that each layer is made up of individual Bi_2Se_3 flakes and the SAED pattern exhibits diffused rings. The diffused rings observed in the electron diffraction indicate the polycrystalline nature of Bi_2Se_3 and they can be indexed to (015) and (110) planes [44,45]. The well-defined morphology of the nanostructured Bi_2Se_3 layers is attributed to the uniform “in core” volumetric heating during microwave irradiation with minimized thermal gradients [22–24]. Bi_2Se_3 -FL have flake like structure possessing very flat surface with uniform height as seen in the AFM images in Fig. S3 (see Supporting information). The thickness of Bi_2Se_3 -FL have been measured and it is approximately 10 nm, suggesting that Bi_2Se_3 -B has been successfully exfoliated into few layers.

Fig. 3 represents the schematic illustration of the formation of stacked layers of Bi_2Se_3 and exfoliation into few layers. Upon mixing the solution of Na_2SeSO_3 and N_2H_4 with $(\text{Bi}(\text{NO}_3)_3 \cdot 5\text{H}_2\text{O})$, the reaction mixture turns dark in color indicating the formation of Bi_2Se_3 flakes at room temperature. The formation of bulk Bi_2Se_3 consisting of individual layers from atomic or molecular scale by chemical reaction follows bottom-up approach [37], whereby microwave irradiation supplies heat energy to the reaction mixture and the individual Bi_2Se_3 flakes move closer to each other and fuse together to form microstructures consisting of few Bi_2Se_3 flakes.

The microstructures thus formed further interact and lead to the

formation of large-sized thin layers of Bi_2Se_3 . The stacking of the layers proceeds along z-axis through covalent bonding involving five atoms in the order of Se–Bi–Se–Bi–Se and this set of five atoms is called one quintuple layer (QL). The individual 2D Bi_2Se_3 layers are held together by weak van der Waals forces giving rise to stacked layers of 3D layered structure [37]. The bulk 3D stacked layers are to be subjected to exfoliation in order to get 2D single-layer or few-layer Bi_2Se_3 by top-down approach as in the case of graphene. Bi_2Se_3 -FL were obtained through sonication assisted liquid-phase exfoliation. During sonication, the mechanical force from sonication is strong enough to overcome the weak van der Waals forces holding the individual Bi_2Se_3 layers, giving way for exfoliation. Each layer of Bi_2Se_3 is made up of several individual Bi_2Se_3 flakes and these exfoliated few-layers possess high surface area to volume ratio, which is advantageous over the bulk 3D material in terms enhanced catalytic activity.

3.2. Electrochemical applications

In this section, inherent electrochemical and the catalytic properties of the nanostructured Bi_2Se_3 -FL are discussed via non-enzymatic glucose sensing.

Fig. 4(A and B) depict the cyclic voltammograms (CVs) recorded for bare glassy carbon (GC) electrode (a) and Bi_2Se_3 -FL modified GC electrode (b) in the absence (A) and in the presence (B) of $\text{K}_3[\text{Fe}(\text{CN})_6]$ in 0.1 M KCl at a scan rate of 0.05 V s^{-1} . The Bi_2Se_3 -FL/GC electrode (Fig. 4(A) curve (b)) shows higher current than the bare GC (Fig. 4(A) curve (a)), owing to the existence of electroactive species (Bi_2Se_3 -FL) on the electrode surface. The cyclic voltammograms recorded for the $[\text{Fe}(\text{CN})_6]^{3-/4-}$ couple for bare GC (Fig. 4(B) curve (a)) and Bi_2Se_3 -FL modified GC (Fig. 4(B) curve (b)) in 0.1 M KCl solution exhibits a reversible electrochemical response for the $[\text{Fe}(\text{CN})_6]^{3-/4-}$ couple (Fig. 4(B) curve (a)), the difference between the redox potential (ΔE_p) of the bare GC electrode in the PBS solution of $[\text{Fe}(\text{CN})_6]^{3-/4-}$ is found to be 70 mV, and the fine peak representing that the bare electrode has excellent conductivity. On introducing Bi_2Se_3 -FL over the surface of GC electrode the peak current is found to increase. Therefore, it is evident that the Bi_2Se_3 -FL/GC stands out to be superior to bare GC, in terms of electron transfer, that can be

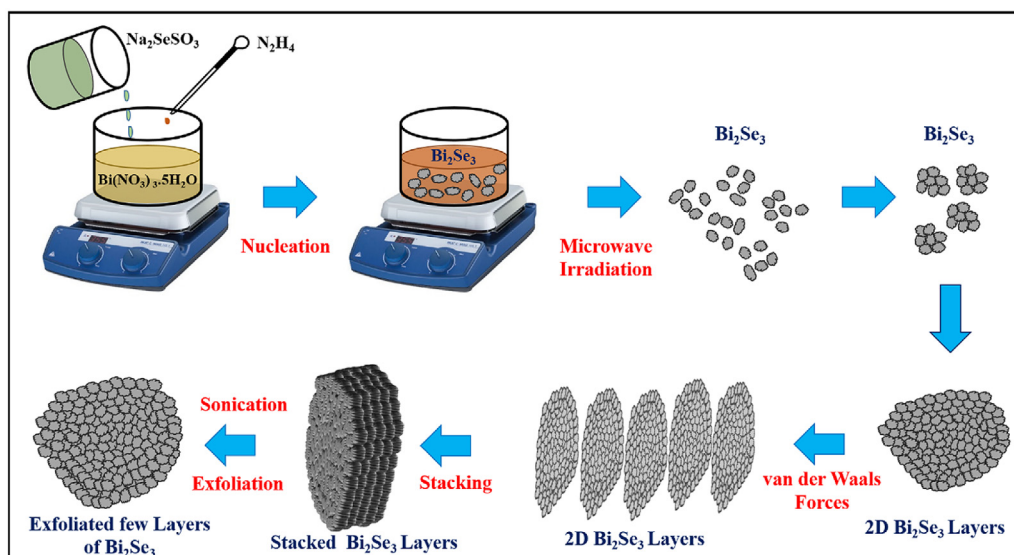


Fig. 3. Schematic illustration of the formation of stacked layers of Bi₂Se₃ and exfoliation Process.

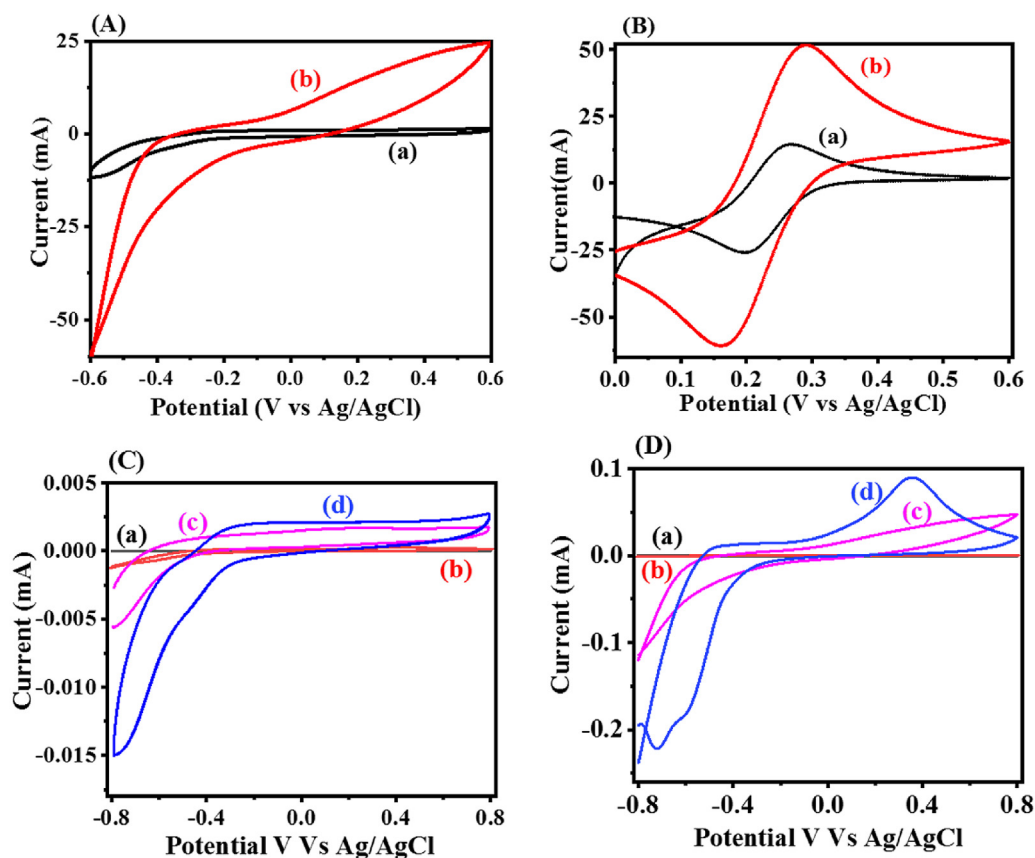


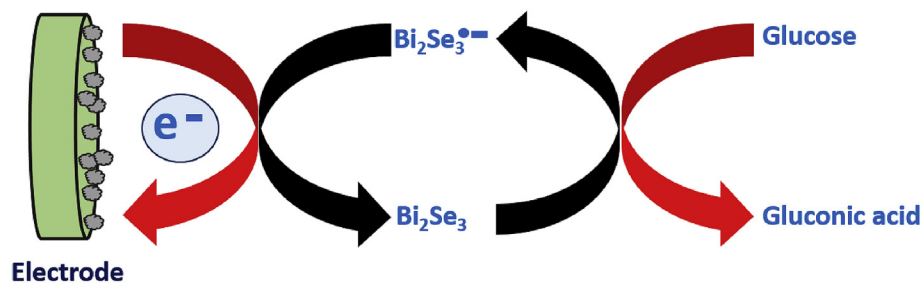
Fig. 4. Cyclic voltammograms recorded for (A) in the absence and (B) the presence of 5×10^{-3} M [Fe(CN)₆]^{3-/4-} in 0.1 M KCl solution recorded for (a) BareGC and (b) Bi₂Se₃-FL/GC electrode; (C) bare GC (a and b) and Bi₂Se₃-Bulk/GC (c and d) in 0.1 M PBS (pH 7.0) in the absence (a and c) and presence (b and d) of 10 mM glucose; (D) bare GC (a and b) and Bi₂Se₃-FL/GC (c and d) in 0.1 M PBS (pH 7.0) in the absence (a and c) and in the presence (b and d) of 10 mM glucose under the optimal experimental conditions. Scan rate: 0.05Vs⁻¹.

attributed to the electrochemically active sites on the surface of Bi₂Se₃ layers which assist the electron transfer process and the high specific area of the Bi₂Se₃-FL. Additionally, the peak separation (ΔE_p) is found to be large for Bi₂Se₃-FL modified GC (125 mV) as compared to bare GC (70 mV), signifying that the electrochemical redox potential in electrode is quasi reversible. This behavior suggest that Bi₂Se₃-FL surface is negatively charged, which is due to the electrostatic repulsion between ferricyanide and surface of Bi₂Se₃-FL [46].

3.2.1. Electrocatalytic oxidation of glucose at the Bi₂Se₃/GC

The electrochemical behavior of Bi₂Se₃-FL/GC towards glucose sensor was examined by cyclic voltammetry technique in a potential ranging from -0.8 to +0.8 V at scan rate 0.05 Vs⁻¹ and compared it with Bi₂Se₃-B/GC. Fig. 4 (C) displays the CVs of the bare GC electrode ((a) and (b)) and Bi₂Se₃-B/GC ((c) and (d)) in 0.1 M PBS (pH 7.0) solution in the absence ((a) and (c)) and in the presence ((b) and (d)) of 10 mM glucose. Similarly Fig. 4 (D) shows the CVs of the bare GC ((a) and (b)) and

compared with that of Bi₂Se₃-FL/GC ((c) and(d)) in the absence ((a) and (c)) and in the presence ((b) and (d)) of 10 mM glucose in 0.1 M PBS (pH 7.0) solution For the bare GC no significant peak is observed in CV both in the presence and absence of 10 mM glucose (curves (a) and (b) in Fig. 4(C) and (D)) in the 0.1 M PBS (pH 7.0). In both the cases, bare GC demonstrated low electrochemical performance than Bi₂Se₃-FL/GC and Bi₂Se₃-B/GC. The comparison of the CV performance of the Bi₂Se₃-B/GC (Fig. 4 (C), curve (a)) with Bi₂Se₃-FL/GC (Fig. 4(D), curve (c)), in the



absence of the glucose, revealed Bi₂Se₃-FL/GC electrode had a superior performance over Bi₂Se₃-B/GC electrode by exhibiting a very sharp peak with current of 9.25×10^{-4} A in the presence of glucose (d) which is ~ 3 and 9 times higher than that of the Bi₂Se₃-FL modified GC in the absence of glucose (Fig. 4 (D) curve (c)) and the bare GC in the presence of glucose (Fig. 4 (D) curve (b)), respectively. The high peak potential exhibited by the Bi₂Se₃-FL/GC electrode evidences for the well-defined electrocatalytic feature of the Bi₂Se₃ to direct oxidation of the glucose in the PBS solution. Therefore, Bi₂Se₃-FL/GC is chosen for the sensing application over Bi₂Se₃-B/GC while bare GC was retained for comparison.

Fig. 5, (A) presents the results of the typical linear sweep voltammetry (LSV) obtained for both bare GC (a) and Bi₂Se₃-FL/GC (b) in 0.1 M PBS (pH 7.0) solution with 10 mM of glucose addition at a scan rate of 0.05Vs^{-1} . It can be seen that the bare GC does not show any oxidation peak current in the presence of glucose (curve (a)), indicating its negligible electrochemical activity for glucose oxidation. On the contrary, Bi₂Se₃-FL/GC demonstrates a strong oxidation peak (curve (b)) at 0.28V and $1.5 \mu\text{A}$ even in the absence of glucose and a very sharp higher oxidation peak current (4×10^{-4} A) with lower oxidation potential (0.19 V) (curve (c)), after adding 1 mM glucose evidences for better electrocatalytic activity of the Bi₂Se₃-FL towards glucose solutions in comparison to bare GC. From

the Electrochemical Impedance Spectroscopy (EIS) it is evident that electro-transfer resistance of Bi₂Se₃-FL/GC electrode is significantly less than that of the bare GC implying that the former can play better role in electrocatalysis than the latter, which is evident from its electrochemical oxidation of glucose (Fig. 5 (B)). The charge transfer resistance (R_{ct}) of the bare GC is 165 Ω , however, after modifying with Bi₂Se₃-FL the electrode's R_{ct} value decreases to 114 Ω , suggesting that Bi₂Se₃-FL is a better medium for electron transfer.

In general, Bi₂Se₃ behaves as an n-type semiconductor due to the charged selenium vacancies which are lattice defects but acting as electron donors [47–49]. The set of five monoatomic layers where the atoms are covalently bonded in the order Se–Bi–Se–Bi–Se, has Se on either side making it almost like a bidentate ligand [18]. During the electrochemical process, Bi₂Se₃ is converted to Bi₂Se₃^{•-} species by one electron trapping process occurring on the surface of Bi₂Se₃ at 0.41 V, which is regenerated upon oxidation at -0.60V . When glucose approaches the surface of Bi₂Se₃^{•-} radical anion it reduces Bi₂Se₃^{•-} to Bi₂Se₃ and glucose gets oxidized in the process. Therefore, Bi₂Se₃ acts as effective electrocatalyst to oxidize glucose and the extent of glucose oxidation is proportional to the current produced. Here Bi₂Se₃ functions as a mediator to enhance the electron transfer between the electrode and glucose and the electrochemical detection of glucose by using Bi₂Se₃ is illustrated by the following equation (1) [50,51].

Fig. 6 (A) exhibits the modified Bi₂Se₃-FL/GC electrode's reaction kinetics examination by recording the influence of different scan rates (ν) while oxidizing glucose. As it is seen in Fig. 6(A), the oxidation peak current increases with the increase in ν value and there is a good linear relationship between the current (i_p) and ν . The plotted relationship verifies that i_p response is linearly proportional to square root of scan rate ranging between 0.01Vs^{-1} and 0.15Vs^{-1} (see Fig. 6(B)). The linear

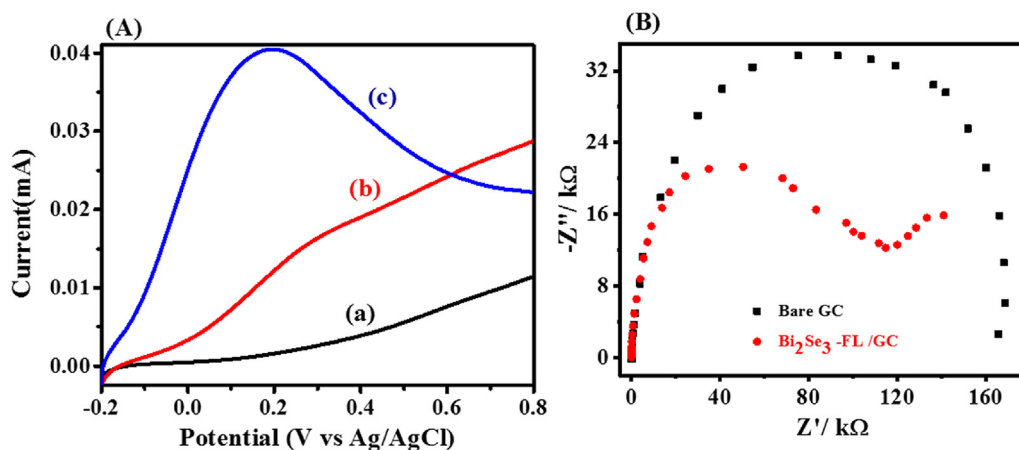


Fig. 5. (A) LSV curves of bare GC (a) and Bi₂Se₃-FL/GC (b and c) in 0.1 M PBS (pH 7.0) in the presence of 10 mM glucose (a and c) and in the absence of glucose (b), under the optimal experimental conditions; (B) Electrochemical impedance spectrum for bare GC and Bi₂Se₃-FL/GC $1.0 \text{mM} [\text{Fe}(\text{CN})_6]^{3-/4-}$ in 0.1 M KCl.

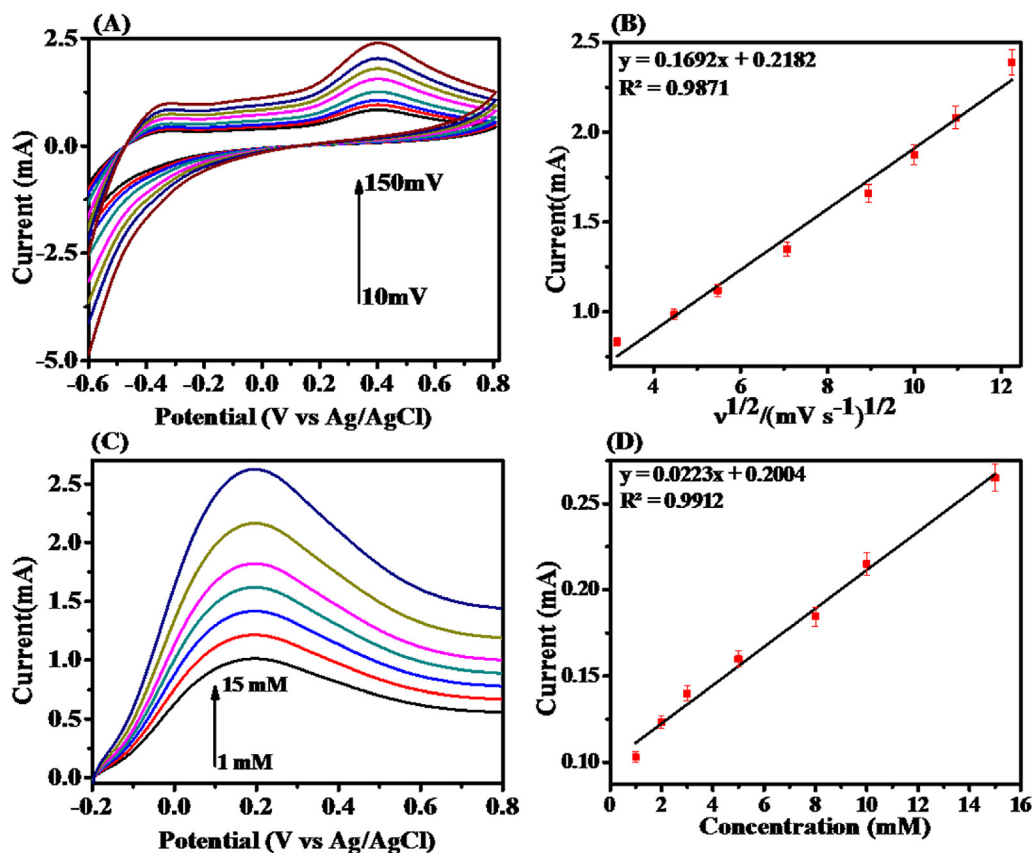


Fig. 6. (A) Cyclic voltammograms for $\text{Bi}_2\text{Se}_3\text{-FL/GC}$ in 1 mM glucose (scan rate 10, 20, 30, 50, 80, 100, 120 and 150 mVs^{-1}); (B) plot of peak current (i_p) vs. square root of scan rate; (C) LSV of $\text{Bi}_2\text{Se}_3\text{-FL/GC}$ electrode with different glucose concentrations: 10, 20, 30, 50, 80, 100 and 150 μM (0.1 M PBS (pH 7.0), scan rate: 0.05 Vs^{-1}); (D) calibration plot of current vs concentration.

relationship between the current vs square root of scan rate represents that it is a diffusion controlled processes ($i_{pa}/\mu\text{A} = 0.1692 \text{ mA}(\text{mVs}^{-1})^{1/2} + 0.2182 \text{ mA}$, $R^2 = 0.9871$). The above consequences specify that the sensor constructed is very stable and a highly reliable electrochemical sensing platform.

As a rapid and appropriate technique for illustrating glucose sensors [52], LSV is employed to explore the electrocatalytic activity of $\text{Bi}_2\text{Se}_3\text{-FL/GC}$ on oxidizing glucose. The LSV of $\text{Bi}_2\text{Se}_3\text{-GC}$ in the presence of different concentrations of glucose in PBS at a scan rate of 0.05 Vs^{-1} is carried out (Fig. 6 (C)). After adding a definite amount of glucose to PBS, a notable anodic peak is accomplished at about 0.19 V. This oxidation peak is due to glucose oxidation and it is confirmed by the addition of different concentrations of glucose. When glucose is added to the PBS solution, the oxidation peak current enormously increases as the concentration of glucose is increased from 1 to 15 mM over a potential range of -0.2 - $+0.8$ V reaching a peak value of $+0.19$ V in 0.1 M PBS solution. Upon the addition of glucose, the oxidation peak current increases linearly. From the calibration plot (Fig. 6 (D)) of current vs concentration, it is clearly seen that there is a linear detection range of 15 mM, while the detection sensitivity is 0.022 mA mM^{-1} with a correlation coefficient (R^2) of 0.9912. The obtained oxidation peak current signals show the important catalytic activity of $\text{Bi}_2\text{Se}_3\text{-FL/GC}$ in its response to glucose. This demonstrates that the $\text{Bi}_2\text{Se}_3\text{-FL/GC}$ is a promising candidate in improving the analytical ability of sensing glucose.

Fig. 7 (A) shows the amperometric response of bare GC (a) and $\text{Bi}_2\text{Se}_3\text{-FL/GC}$ (b) at 0.19 V with successive additions of glucose into 0.1 M PBS (pH 7.0) solution at constant intervals. The electrode displays a quick response when glucose is added, and the time to attain 96% steady-state current is not more than 3s, representing a very rapid and good response for glucose. The corresponding calibration plots for the electrodes over the glucose concentration range of 10–100 μM are presented in Fig. 7(B).

The current response has linearly increased on increasing glucose concentration, as shown in the calibration plot (current vs glucose concentration) of amperometric response in Fig. 7 (B). The calibration plot is found to be linear with a correlation coefficient (R^2) of 0.9921. The regression equation $y = 0.112x - 0.071$ with the lower detection limit (LOD) is observed to be as low as 6.1 μM at the signal-to-noise ratio (S/N) of 3. Additional, sensitivity is calculated as 0.112 $\mu\text{A}\mu\text{M}^{-1}$ by dividing the slope of the linear portion of calibration plots with electrode surface area. The improved sensing performance of non-enzymatic glucose sensor attributed to $\text{Bi}_2\text{Se}_3\text{-FL/GC}$ electrode is because it offers high surface area, resulting in rapid electron transfer through electrochemical process for the oxidation of glucose occurring between the electrolyte and electrode. The results obtained here evidence the feasibility to fabricate $\text{Bi}_2\text{Se}_3\text{-FL}$ based non-enzymatic glucose sensor with sufficient stability, sensitivity, selectivity and with good reproducibility. To support our claim further we have compared this work with other recently published works on non-enzymatic glucose sensors and presented in Table S1 (see supplementary information). [S1-S8].

3.2.2. Interference analysis, repeatability and reproducibility of the $\text{Bi}_2\text{Se}_3\text{-FL/GC}$ modified electrode

In addition to sensitivity, selectivity and anti-interference are the other significant features expected of high-performance non-enzymatic glucose biosensors as poor selectivity and interference of other species can bring down the performance of the device. Hence sensitivity and anti-interference capacity of the $\text{Bi}_2\text{Se}_3\text{-FL/GC}$ electrode was evaluated and presented here. Fig. 8 shows, the selectivity of $\text{Bi}_2\text{Se}_3\text{-FL/GC}$ electrode toward glucose sensing in the presence of different interfering species such as ascorbic acid (AA), dopamine (UA), uric acid (DA), and sucrose. The detection is demonstrated using the amperometric response of the electrode sensing with the adding of 2 μM glucose and 2 μM of each

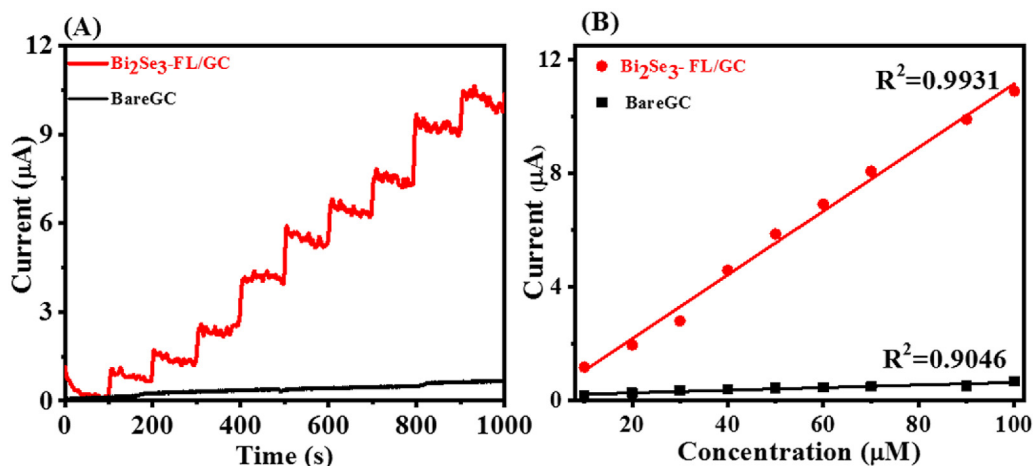


Fig. 7. (A) Amperometric current–time (*i*-*t*) curves to the successive addition of glucose in 0.1 M PBS (pH 7.0) at constant potential: 0.19 V. (B) The corresponding calibration curve current versus concentration of glucose.

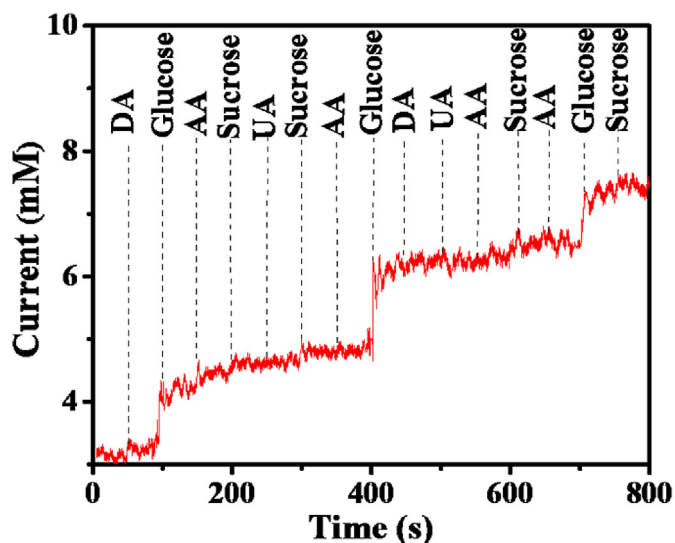


Fig. 8. Amperometric responses of Bi₂Se₃-FL/GC to successive additions of 2.0 μM glucose and 1.0 μM UA, AA, DA and Sucrose in 0.1 M PBS (pH 7.0) at 0.19 V.

of the above interfering analytes in a solution of PBS (0.1 M) at +0.19 V (vs Ag/AgCl). It can be seen that, after each addition of glucose the current response raises; whereas when interfering analytes are added negligible current responses are observed. The above results suggest that the fabricated Bi₂Se₃-FL/GC electrode can be used for selective detection of glucose and also for the determination of glucose in real samples under physiological conditions.

The stability of the Bi₂Se₃-FL/GC sensor is observed by analyzing its response of current to glucose over 19 days. After 19 days, only 17% loss in current signal is detected from its initial response (see Figs. S4(A) and S4(B) in supplementary information). The excellent stability of modified electrode can be ascribed to the stability of Bi₂Se₃-FL. To examine the reproducibility of the Bi₂Se₃-FL/GC sensor towards the electrocatalytic oxidation of glucose, five freshly prepared electrodes were assessed by associating their current responses in 0.1 M PBS containing 10 mM glucose at the scan rate of 50 mVs⁻¹ (Fig. S4(C) and S4 (D) in supplementary information). A relative standard deviation (RSD) of 2.4% is obtained, indicating the reliability of the method and material. A set of 5 measurements for a distinct electrode was made upon the addition of 10 mM glucose in 0.1 M PBS, and it resulted in 3.1% of RSD, demonstrating excellent reproducibility. Likewise, the repeatability Bi₂Se₃-FL/GC

electrode is measured using 6 models separately, by adding 10 mM of glucose at 50 mVs⁻¹ scan rate (see Figs. S4(E) and S4 (F) in supplementary information). After 6 times usage, Bi₂Se₃-FL/GC glucose sensing electrode retained around 94% of its original response, exhibiting outstanding reproducibility and repeatability of non-enzymatic glucose sensing ability.

3.2.3. Real sample analysis

The outstanding detecting performance of Bi₂Se₃-FL/GC electrode suggests its appropriateness for glucose detection in real samples, which was examined by detecting the glucose present in the urine sample collected from a healthy volunteer. The human participants were informed of the consents. The glucose concentration was detected at the Bi₂Se₃-FL/GC in the presence of 100 μL of urine. For all the tests, standard glucose was added to calculate the recovery rate, and the Bi₂Se₃-FL/GC sensor displayed a good recovery in between 96.0 and 101.2%, with a fine RSD value of 2.3% (n = 3) [53,54]. These results obtained strongly suggest that the Bi₂Se₃-FL/GC has noticeable potential application in repetitive glucose sensing, with promising precision and accuracy Table S2 (see supplementary information).

4. Conclusion

In summary, we have successfully developed Bi₂Se₃-FL based non-enzymatic electrochemical glucose sensor. The individual Bi₂Se₃ layers are made up of small Bi₂Se₃ flakes which result in larger surface area and exhibit Localized Surface Plasmon Resonance (LSRP) because of cation vacancy exhibited enhanced electrocatalytic activity. The experimental results obtained demonstrated that Bi₂Se₃-FL/GC electrodes possess excellent electrocatalytic activity towards the oxidation of glucose and upon glucose addition, the system reached steady-state level within 3 s. The interface showed a linear behavior from 10 μM to 100 μM of glucose concentration, with a current sensitivity of 0.112 μAμM⁻¹ and a detection limit of 6.1 μM. The Bi₂Se₃-FL based glucose sensors exhibited fast response, high sensitivity and good stability towards the oxidation of glucose. All these results suggest that the proposed sensor is an attractive and effective tool for practical glucose monitoring and opens a new avenue to explore the potential applications of Bi₂Se₃ in the field of electrochemical biosensors/sensors.

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Appendix A. Supplementary data

Supplementary data to this article can be found online at <https://doi.org/10.1016/j.jelechem.2019.113629>.

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